



Imaging and Radiotherapy with Synchrotron X-rays

Rob Lewis



Other Modalities

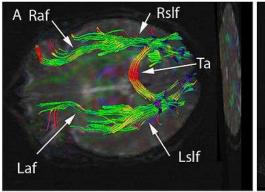
Ultrasound

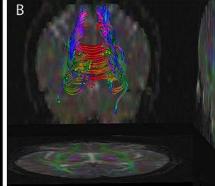
- **✓** Cheap
- ✓ No radiation dose
- Cannot penetrate bone or air
- Spatial resolution degrades with depth
- Scan times are minutes

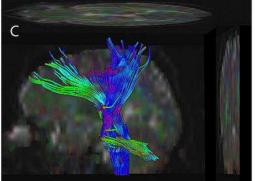
MRI

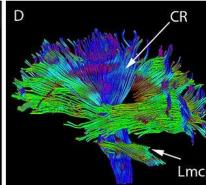
- ✓ Fantastic soft tissue contrast
- ✓ Minimal radiation dose
- **Expensive**
- Scan times are many minutes
- Spatial resolution f(B)







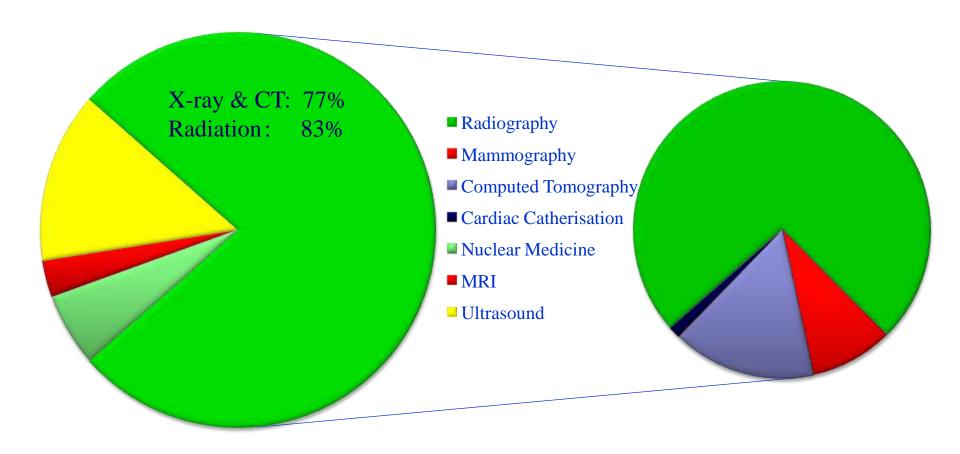








Diagnostic Imaging in Canada



Source: Canadian MIS Database, Candian Institute for Health Information 2007 with thanks to Paul Babyn



MRI

- Cost:
 - **◆ CT:** From \$700 to \$2,200
 - **♦ MRI:** From \$1200 to \$4000
- Time taken for complete scan
 - ◆ CT: Usually completed within 5 minutes
 - **♦ MRI:** Typically 30-40 minutes

MRI Accidents





MRI-CT Comparison

CT MRI



MRI-CT Comparison

CT MRI



Current Trends

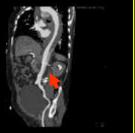
- Preventative medicine is a good idea
- Medical imaging procedures can detect disease at a stage when it can be treated effectively
 - ◆ Funding bodies (public and private) will fund imaging procedures
- There is a trend towards more imaging, particularly screening
 - **♦** Mammography
 - Whole body CT scans
- Screening means go fast!



e lumen, very sharp







SOMATOM Definition Flash

Flash speed. Lowest dose.

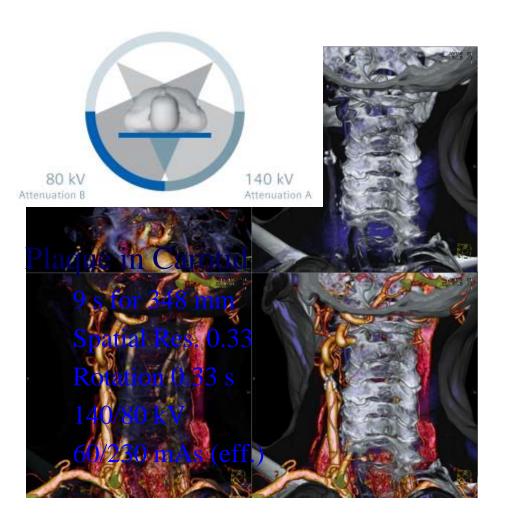
collimation: 128 x 0.6 mm spatial resolution: 0.33 mm

scan time: 2.3 s scan length: 613 mm rotation time: 0.28 s 100kV, 183 effective mAs

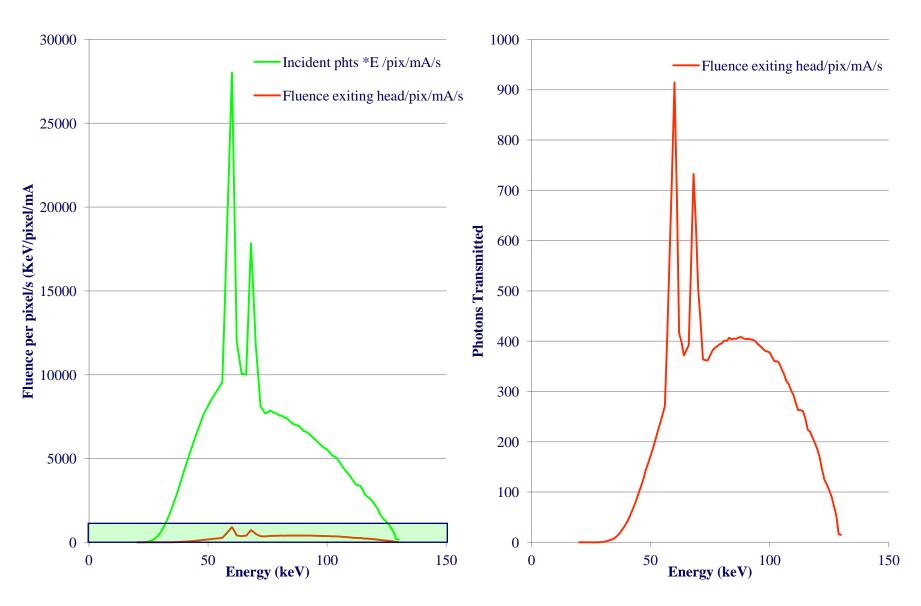
6.2 mSv

Courtesy of Centre Cardio-Thoracique de Monaco / Monaco

Dual Energy CT



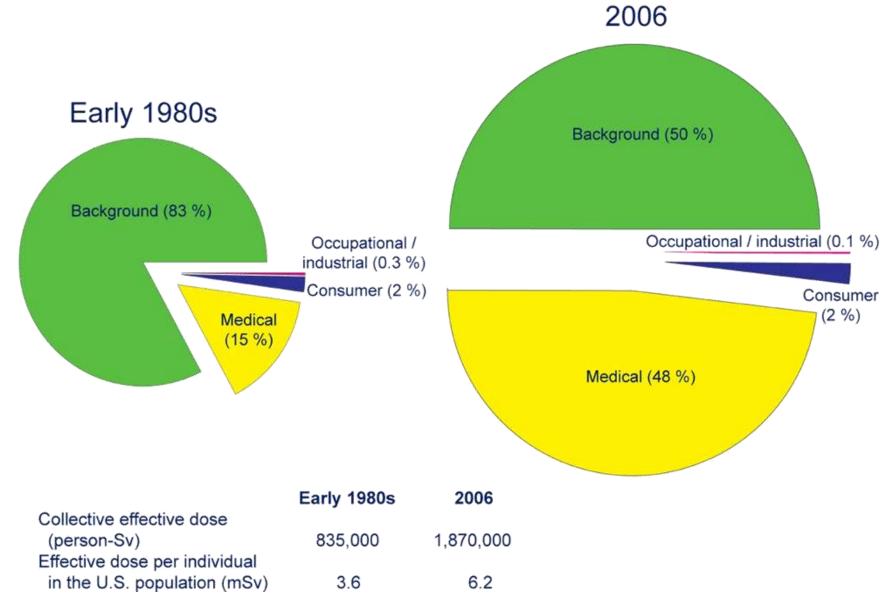
Fluence and Dose



What is the Risk from Radiation?

- A lifetime dose of 100mSv increases cancer risk by ~1%
 - ♦ 1000 chest x-rays
 - ♦ 100 mammograms
 - ♦ 50 head CT scans
 - ♦ 10 abdominal or pelvic CT scans
- Background Dose is ~ 2.4mSv/year
- On 31 May, Fukushima prefecture dose rate was 1.5µSv/h
- It takes most radiation-induced cancers 10 to 20 years to develop in adults
- The average lifetime risk of developing cancer is 42%
- From early 1980s to 2006, 7× increase in population dose from medical procedures

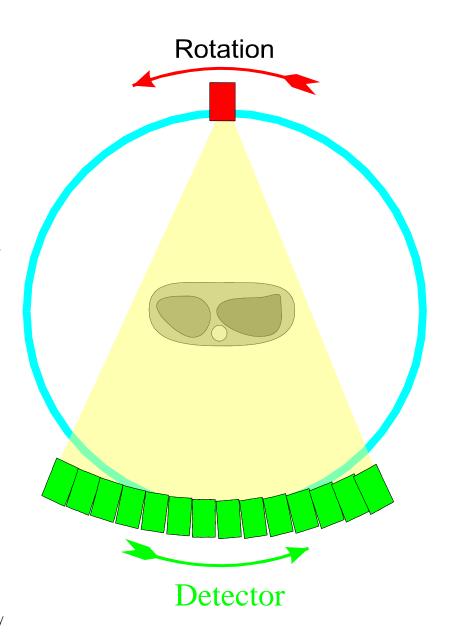
Trends in Radiation Dose from Medical Imaging



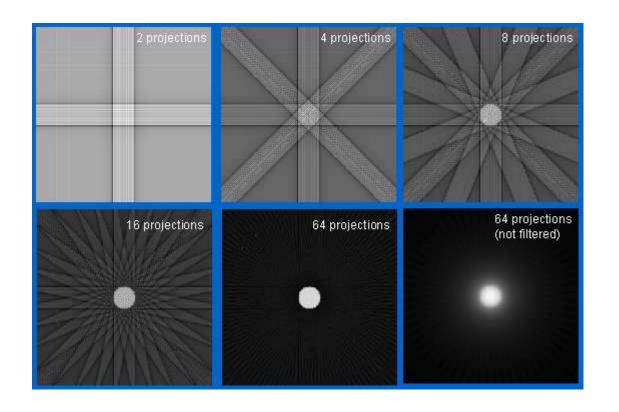


3rd Generation CT Scanner

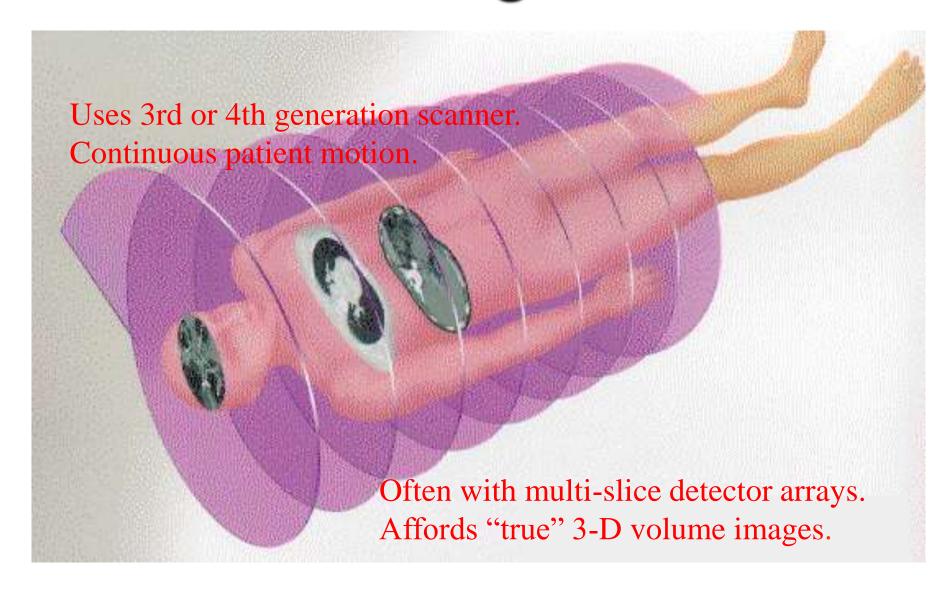
- Multiple detectors
- Translation-rotation
- Large fan beam
- Patient stationary for each
 2-D slice acquisition;
 about 0.1 seconds per slice
- kV = 120, mA = 500
- Image then reconstructed in about 0.1 seconds



FBP in Practice



Volume CT image



Beam Harding Artefacts

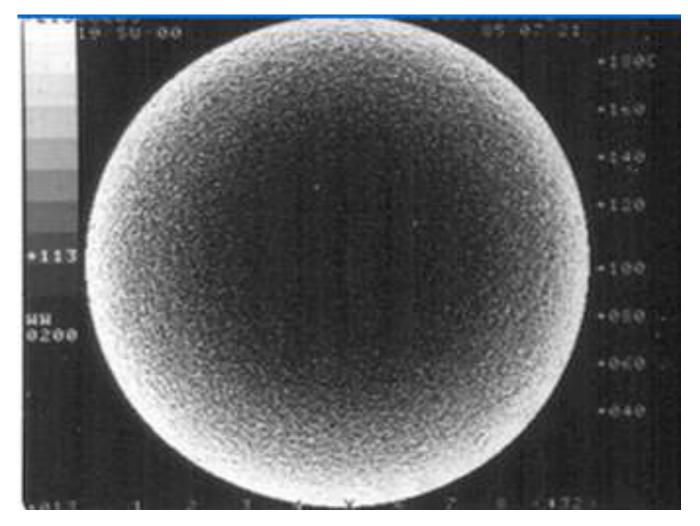
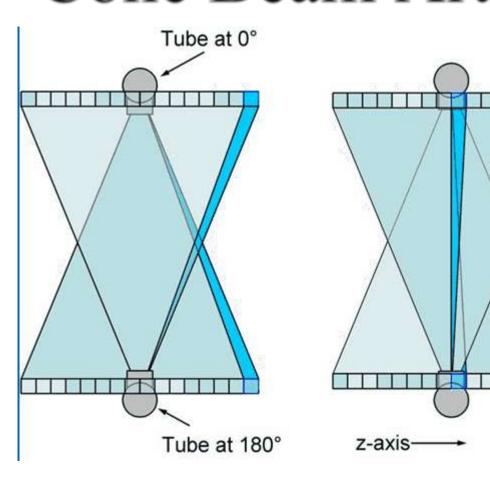
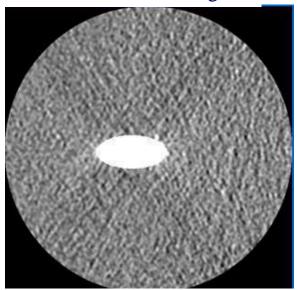


Image of uniform phantom

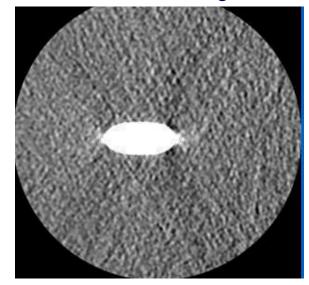
Cone Beam Artefacts



Inner detector row image



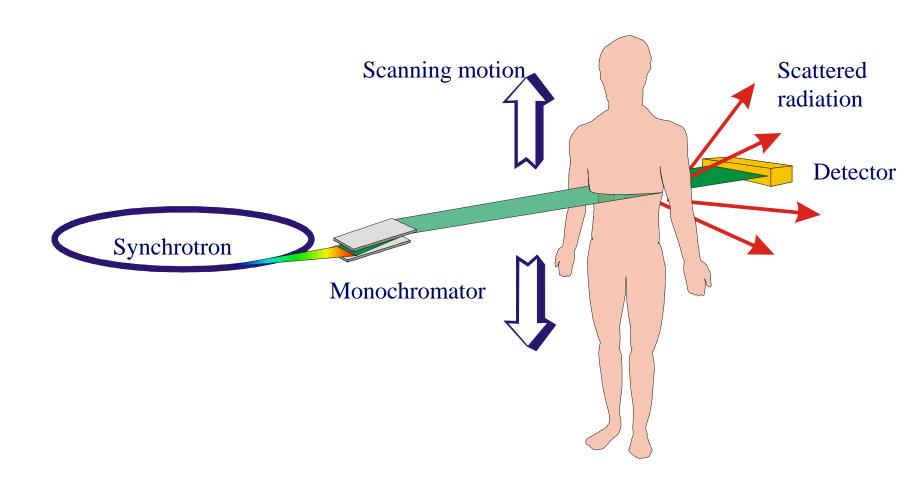
Outer detector row image



Exploit What Synchrotrons Are Good At

- Synchrotron is a great tool for performing medical physics studies
 - ♦ Synchrotron beams can be monochromated
 - No beam hardening
 - ♦ Synchrotron beams are almost parallel
 - No cone beam artefacts
 - Scatter removal with no dose penalty
- Allows studies of better x-ray imaging and developing new methodologies

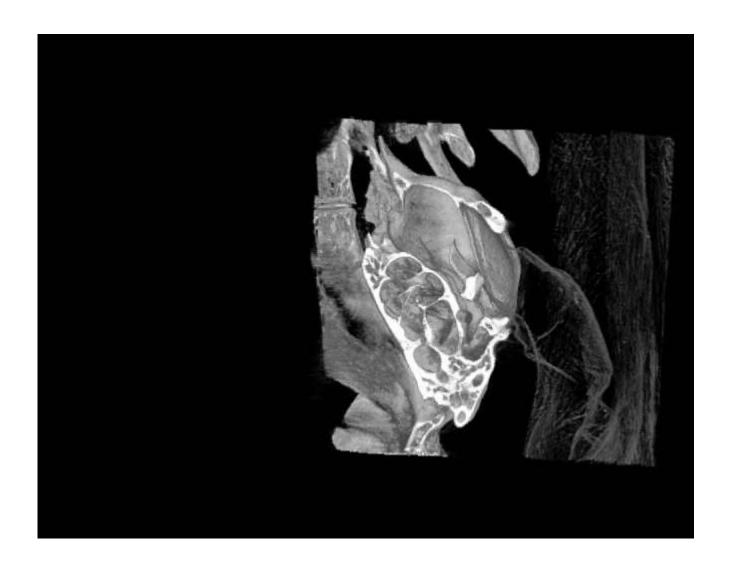
Synchrotron Radiography



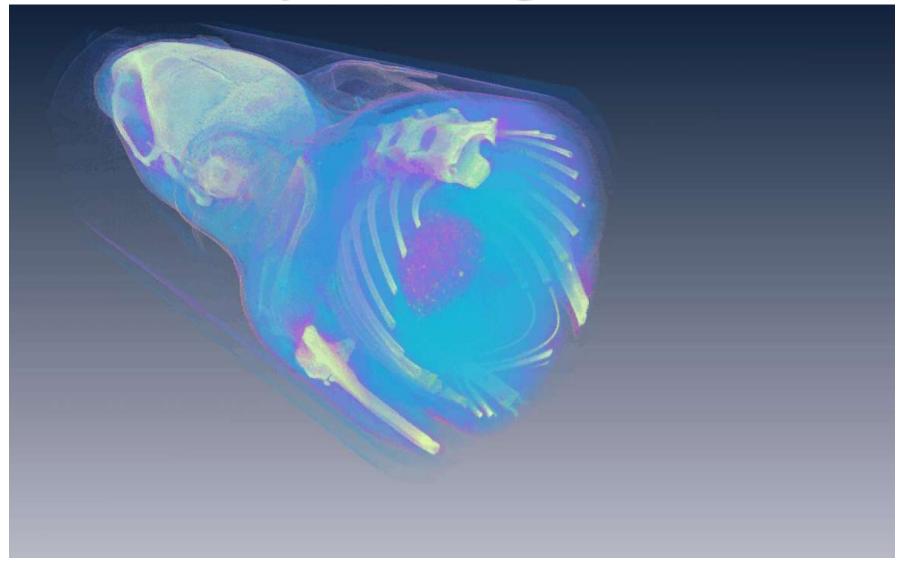
Mouse CT



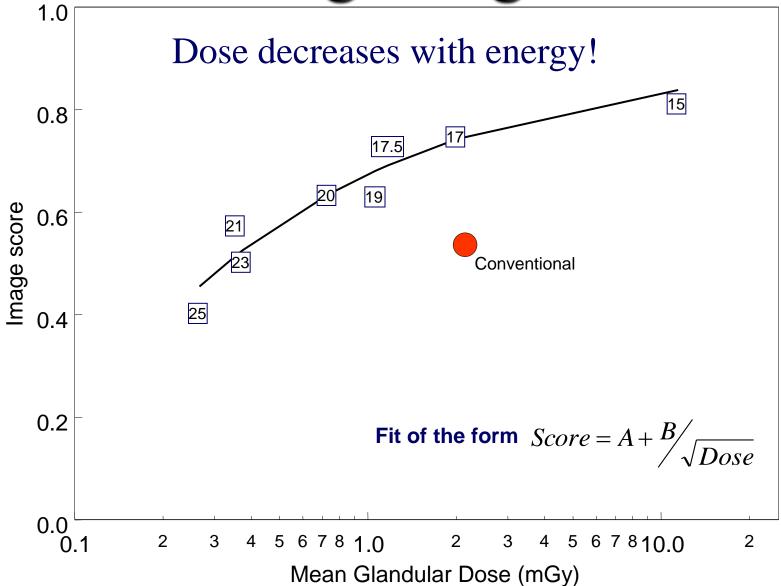
Mouse Cochlea



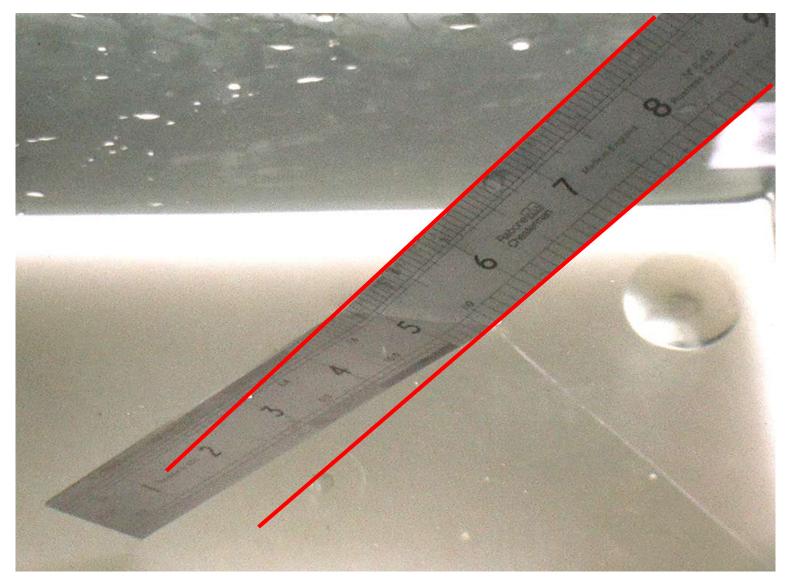
Mouse Fly Through



Slot Scanning Image Scores

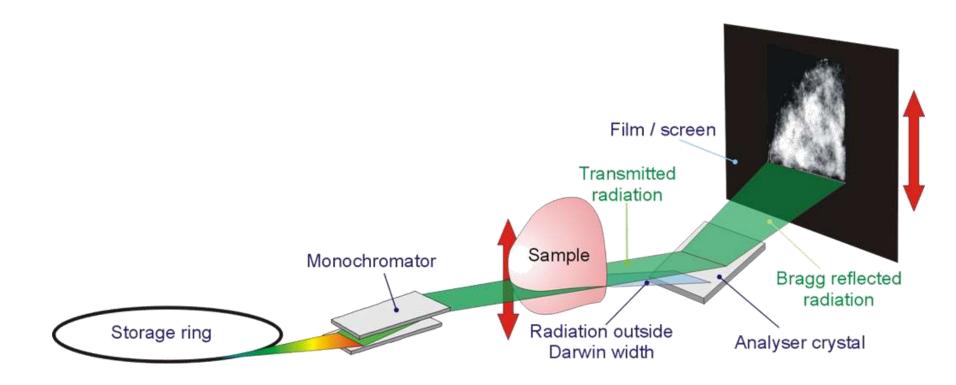


Refraction

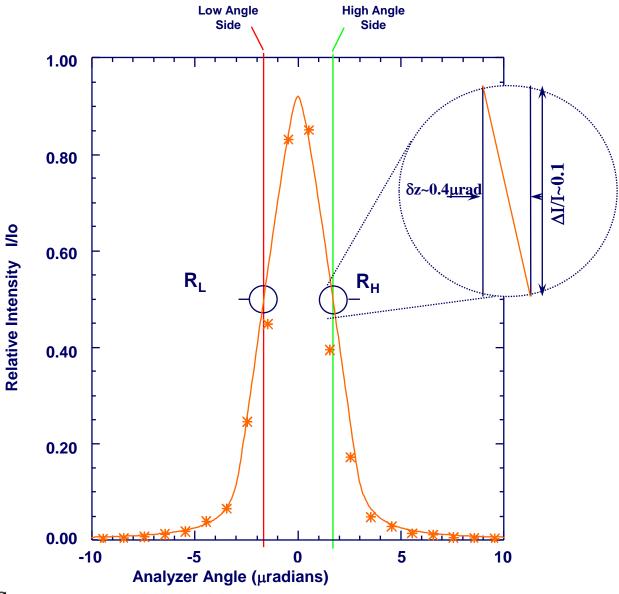


Analyser Based Imaging

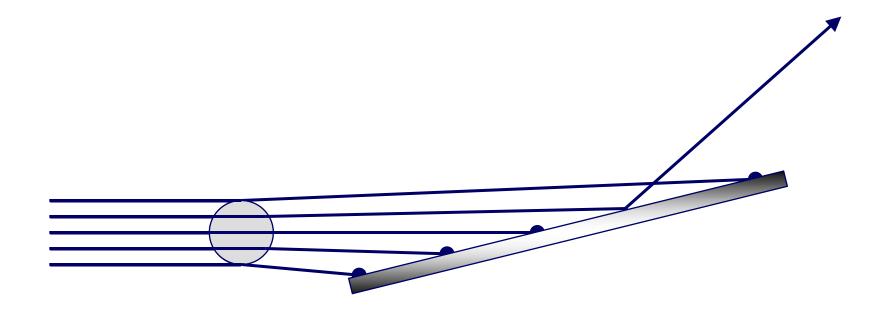
Sometimes called Diffraction Enhanced Imaging



Crystal Rocking Curve

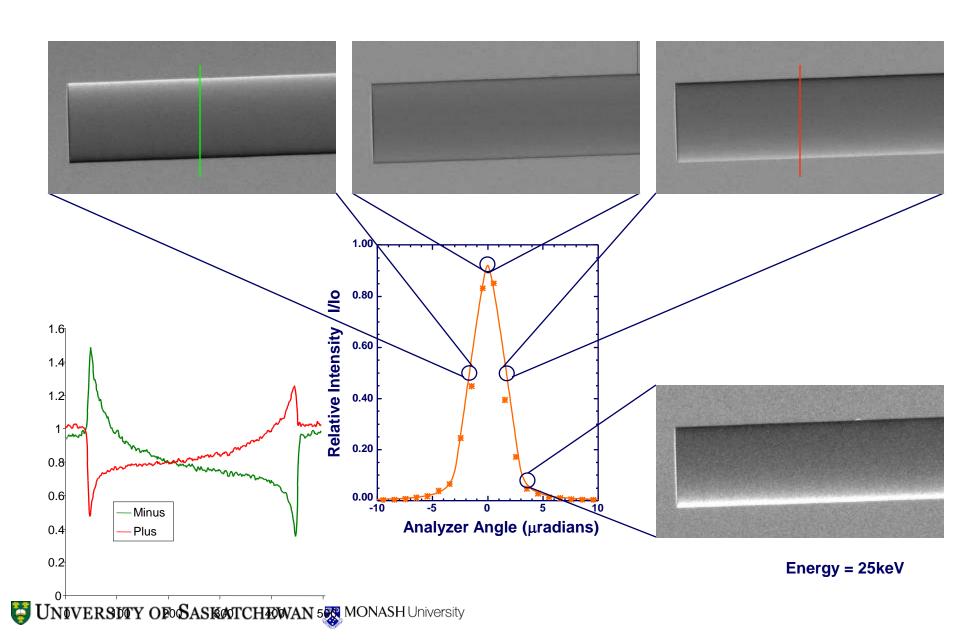


Rocking Curve



Refractive index for X-rays is less than 1 by about 1 part in a million

ABI How it works



ABI Mathematics

- I_L & I_H = Intensities on low and high angle sides of rocking curve
- Grad_L & Grad_H =
 Gradients of low and high
 angle sides of rocking
 curve

- \blacksquare I_R is intensity
- $\Delta \theta_z$ = refraction angle

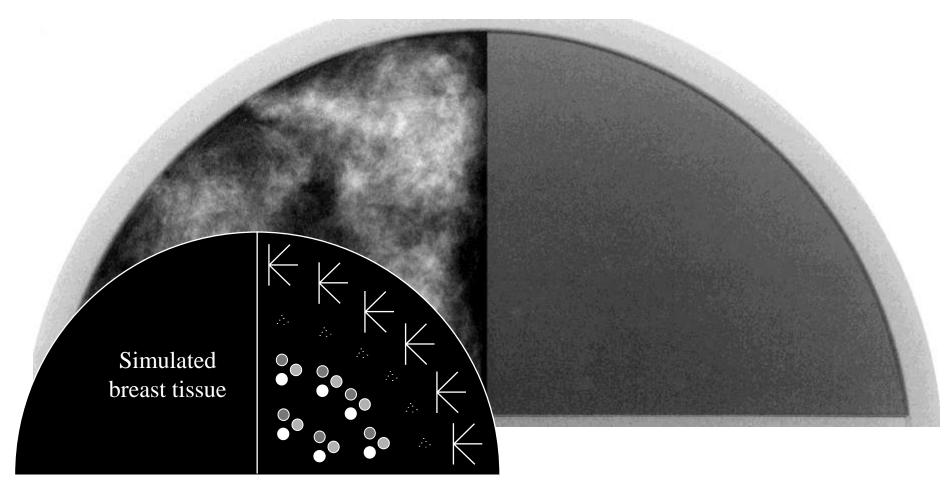
Given

$$I_{L} = I_{R} \cdot (R_{L} + Grad_{L} \cdot \Delta \theta_{Z})$$

$$I_{H} = I_{R} \cdot (R_{H} + Grad_{H} \cdot \Delta \theta_{Z})$$

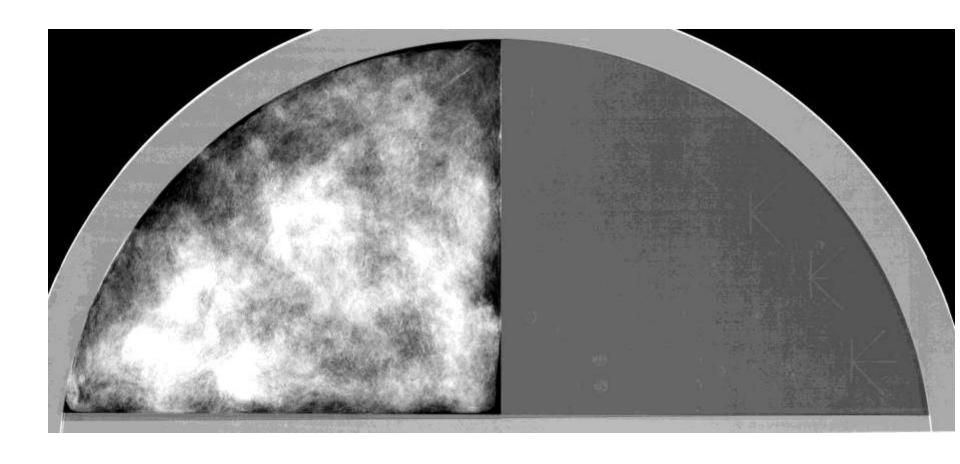
$$\operatorname{Find}(I_{R}, \Delta\theta Z) \rightarrow \begin{pmatrix} \operatorname{Grad}_{H} \cdot I_{L} - \operatorname{Grad}_{L} \cdot I_{H} \\ \overline{\operatorname{Grad}_{H} \cdot R_{L} - \operatorname{Grad}_{L} \cdot R_{H}} \\ \\ \underline{I_{H} \cdot R_{L} - I_{L} \cdot R_{H}} \\ \overline{\operatorname{Grad}_{H} \cdot I_{L} - \operatorname{Grad}_{L} \cdot I_{H}} \end{pmatrix}$$

TORMam Conventional



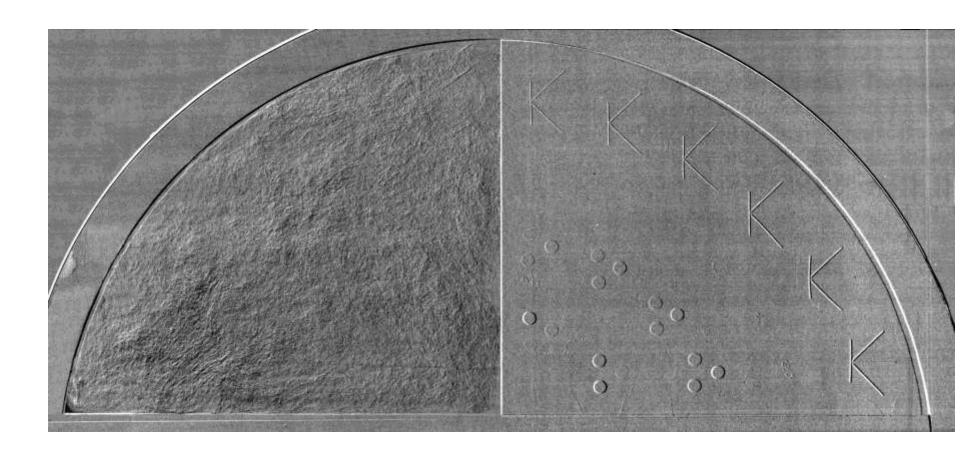
Spectrum = Mo:Mo 28kVp

TORMAM Peak



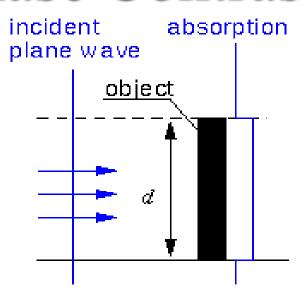
Energy = 20keV

TORMAM Refraction



Energy = 20keV

Phase Contrast



$$N_F = \frac{d^2}{\lambda_7}$$

z=0

Contact:

 $N_F >> 1$ Geometric approximation

♦ The intensity distribution is a pure absorption image.

■ Near field:

 $N_F >> 1$ Geometric approximation

♦ Contrast is given by sharp changes in the refractive index, i. e. at interfaces.

■ Intermediate field: $N_F \sim 1$ Fresnel approximation

♦ The image loses more and more resemblance with the object.

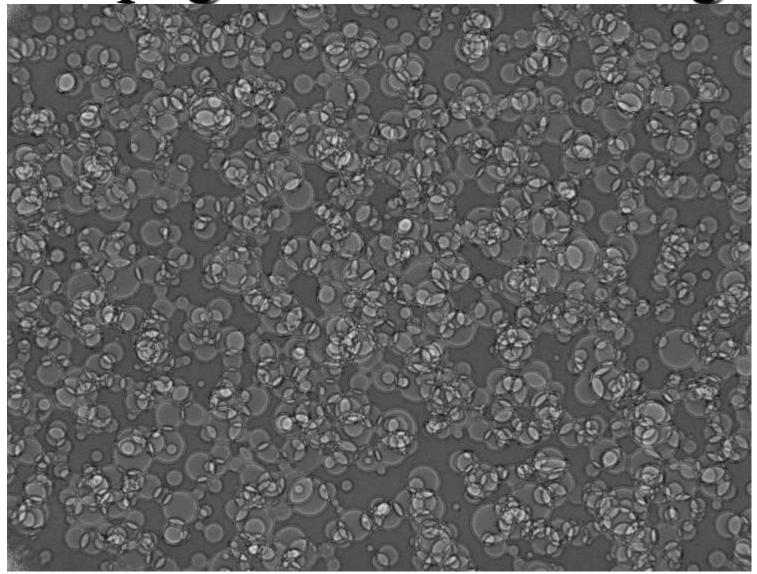
■ Far field:

 $N_F \ll 1$ Far: Fraunhöfer approximation

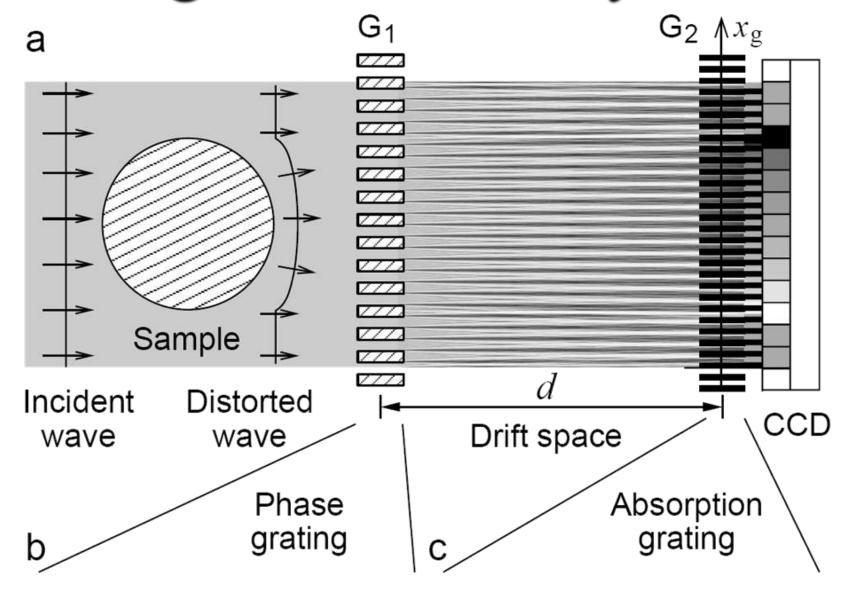
The image is the Fourier transform of the object transmission function

Propagation Based Imaging

147cm



Grating Interferometry





Grating Imaging: Mouse Embryo

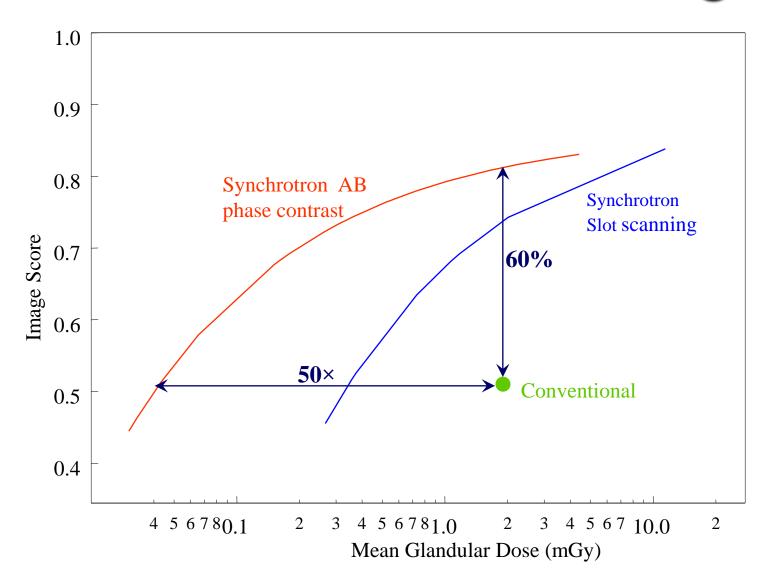


Exploit What Synchrotrons Are Good At

- Synchrotrons allow fantastic spatial resolution
- But what about the dose?

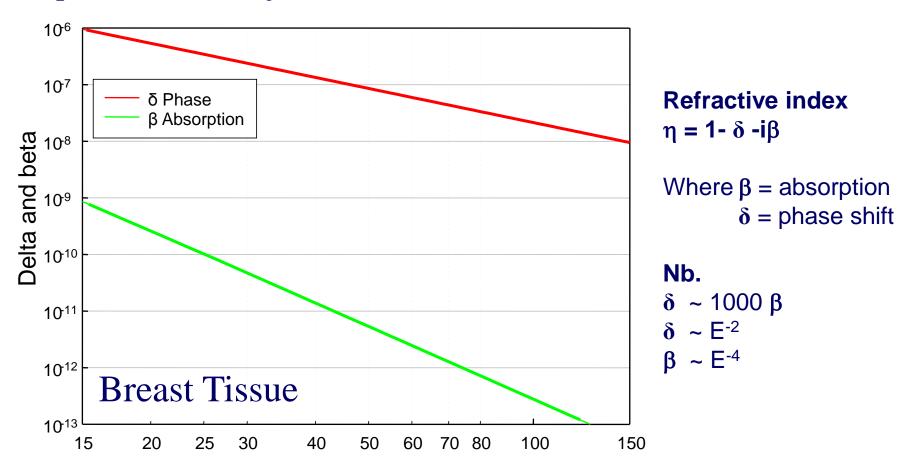
$$Dose_{skin} = \frac{2e^{\mu L}SNR_{out}^{2}}{DQE(f)\mu^{2}size_{obj}^{4}Contrast_{\mu}^{2}}E_{\gamma}(\frac{\mu}{\rho})$$

Phase Contrast Dose Advantage



Complex Refractive Index

- Coherence properties enable phase contrast
- Contrast arising from phase effects does not require dose to be deposited in the object





CT and Radiography Problems

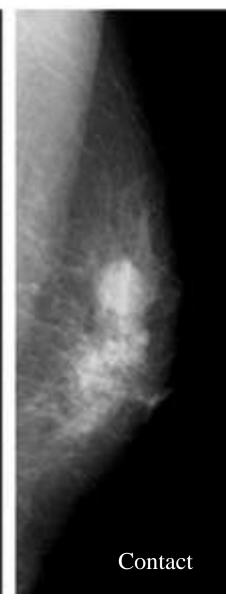
- X-ray Dose
 - Phase Contrast Helps. Synchrotron easy. Gratings?
- Scatter
 - Greatly reduced by slot scanning. Both conventional and synchrotron can use this.
- Beam Hardening
 - Eliminated by monochromatic radiation. Synchrotron only
- Cone Beam Artefacts
 - Eliminated by parallel beam. Synchrotron only.

Phase Contrast in the Clinic

Konica Minolta REGIUS PureView

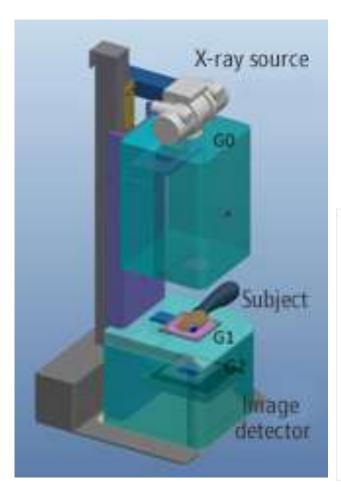






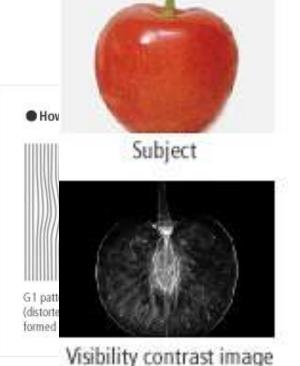
Phase Contrast in the Clinic

Konica Minolta Research & Development



New X-Ray Imaging Technology for Examining Cartilage

Konica Minolta technology has succeeded in imaging cartilage using conventional X-ray sources available in hospitals



Differential phase contrast image

aving the resolution

ating patterns,

stector.

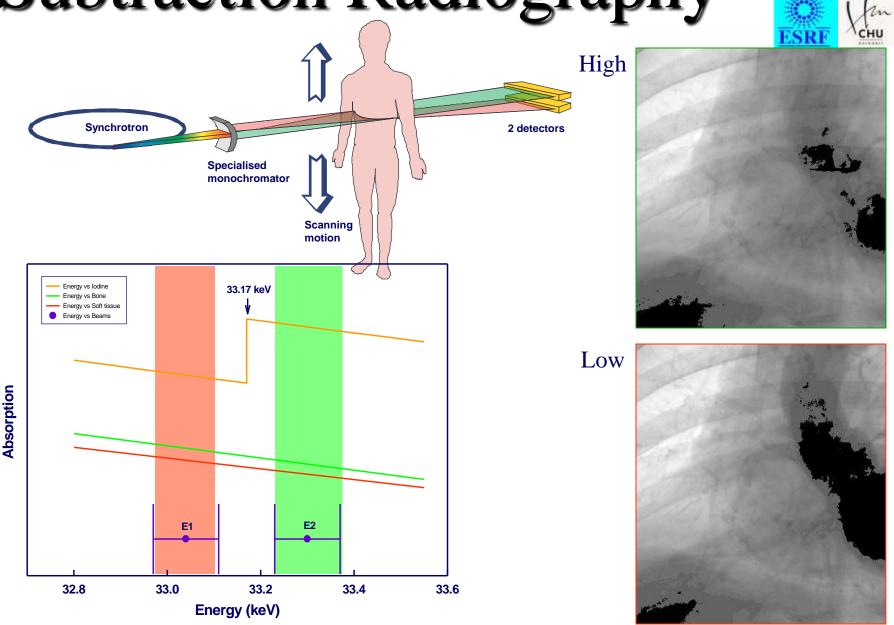
Absorption contrast image

http://www.konicaminolta.com/about/research/ special_healthcare/talbotlau.html





Subtraction Radiography

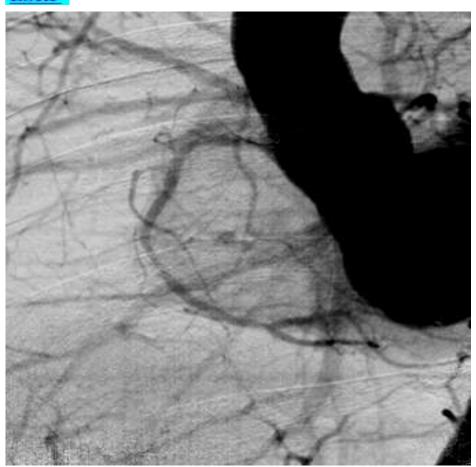


University of Saskatchewan Monash University W. Thomlinson et al ESRF

Patient 1 - weight: 70 kg - iodine: 42ml







Synchrotron IV injection n.b. 2 – LAO 40



Conventional angiography Intra arterial injection

Synchrotron Clinical Studies

- Coronary Angiography
 - ♦ Several hundred patients in Hamburg and at ESRF
 - ◆ Synchrotron sensitivity allowed venous injection rather than arterial as is required in hospital
 - ♦ Not all coronary arteries always visualised well
- Mammography
 - ♦ Clinical program ongoing at Elettra
 - ♦ Preliminary results look encouraging



Synchrotron Medical Imaging

- Synchrotron Medical Imaging
 - ✓ Fantastic spatial resolution
 - ✓ Reasonable scan times
 - **✗** Uses ionising radiation
 - Very limited access
 - **Extremely** expensive
- Synchrotrons are not currently suitable for "routine" medical procedures

Case Study: Birth One of the greatest Physiological challenges

- During fetal life the future airways of the lungs are liquid-filled
- At birth lungs must rapidly transform from being liquid to air filled
- How this happens is poorly understood but the process
 - Develops late in pregnancy
 - ♦ Is initiated by labour
- Preterm and caesarean section infants often develop problems
 - ♦ Incidence is increasing
 - ♦ Require weeks of assisted ventilation (>\$2,000/day)
- We know that ventilating infants causes injury
 - ♦ ~30% develop chronic lung disease
 - ♦ Becomes apparent after 15 years

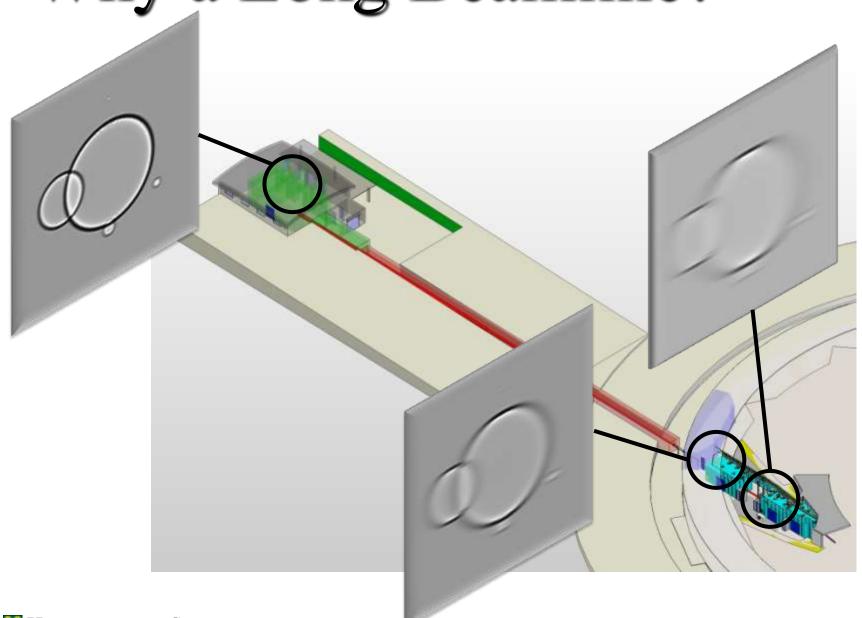


SPring-8 - Super Photon ring-8GeV

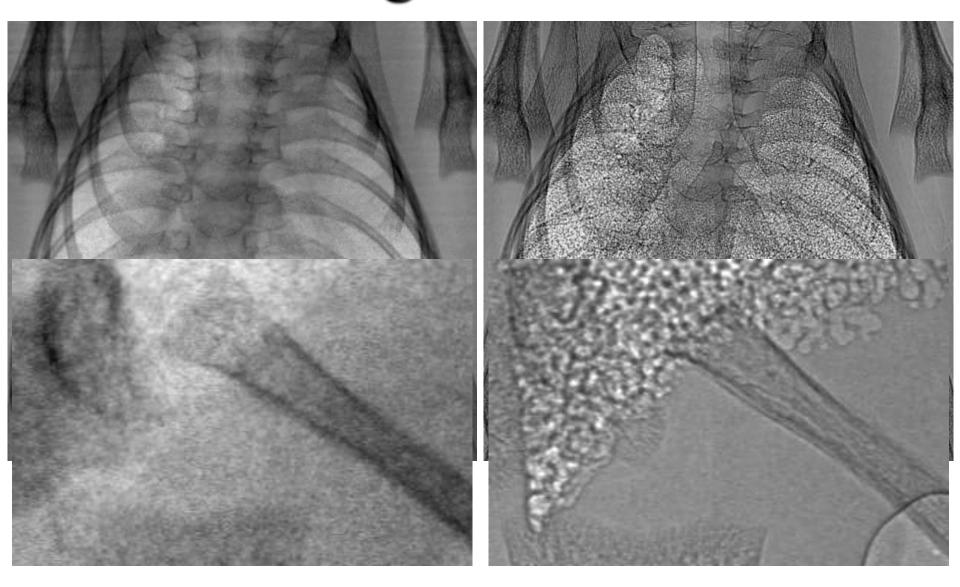


SACLA SPring-8 Angstrom Compact Free Electron Laser

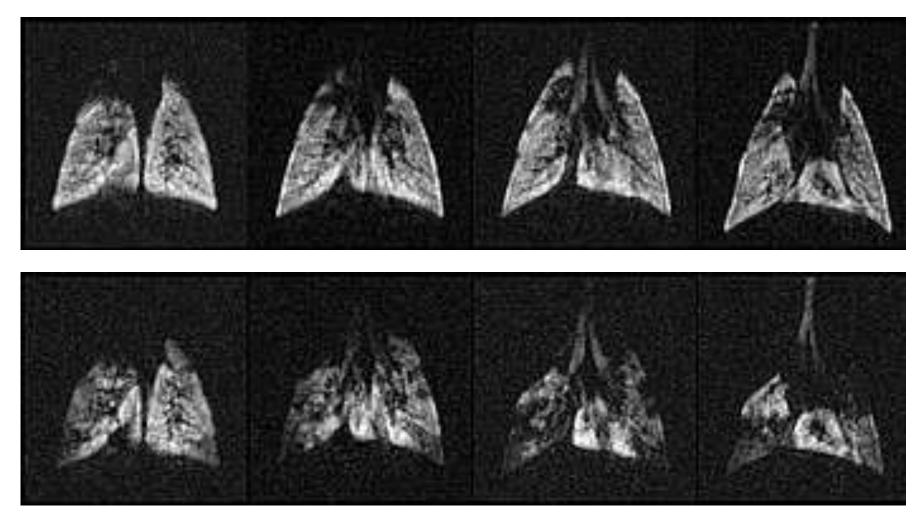
Why a Long Beamline?



Rabbit Lung

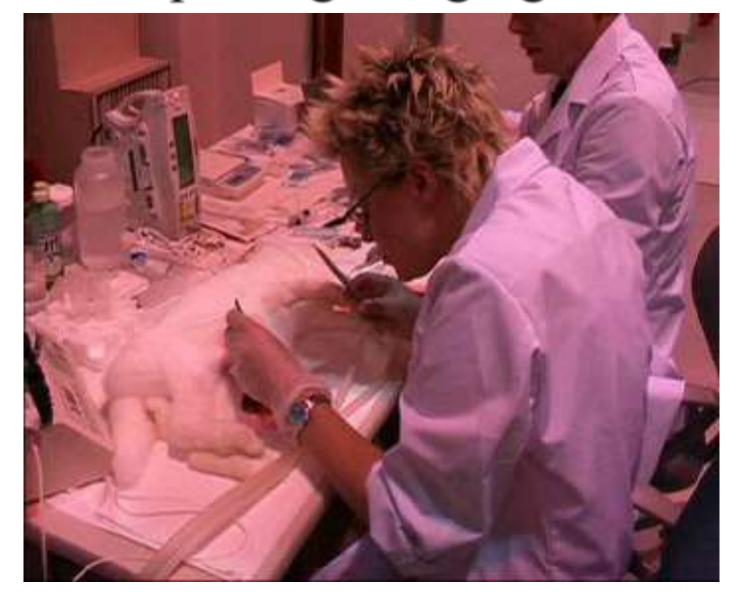


MRI State of the Art

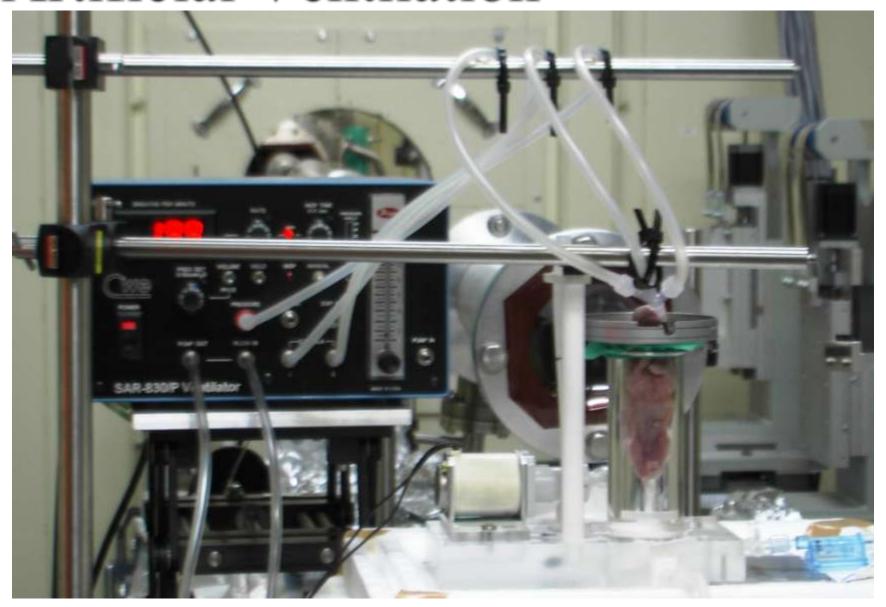


Bronchoconstriction induced by metacholine

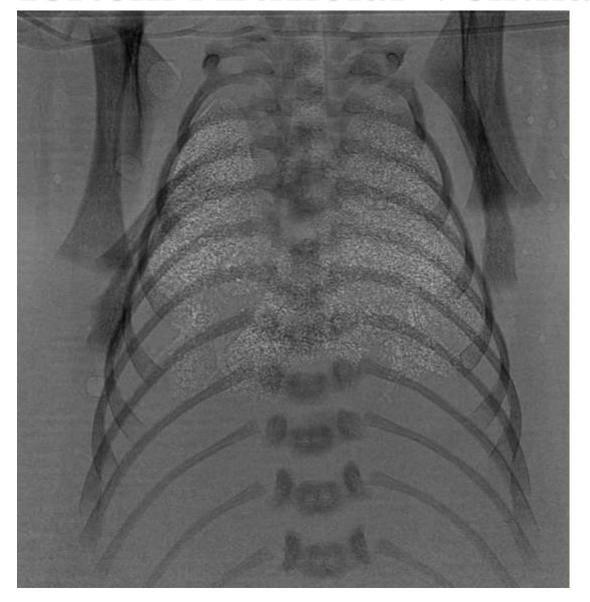
Rabbit Pup Lung Imaging - Delivery



Artificial Ventilation



Post Mortem Artificial Ventilation



Phase Retrieval: Single Image

Approximate 'contact' intensity from Beer's Law

$$I(\mathbf{r}_{\perp}, z = 0) = I_O \exp(-\mu T(\mathbf{r}_{\perp}))$$

Approximate 'contact' phase by

$$\phi(\mathbf{r}_{\perp}, z=0) = -\frac{2\pi}{\lambda} \delta T(\mathbf{r}_{\perp})$$

 $\phi(\mathbf{r}_{\perp}, z = 0) = -\frac{2\pi}{\lambda} \delta T(\mathbf{r}_{\perp})$ Use Transport-of-Intensity Equation (TIE)

$$\nabla_{\perp} \cdot (I(\mathbf{r}_{\perp}, z) \nabla_{\perp} \phi(\mathbf{r}_{\perp}, z)) = -\frac{2\pi}{\lambda} \frac{\partial}{\partial z} I(\mathbf{r}_{\perp}, z)$$

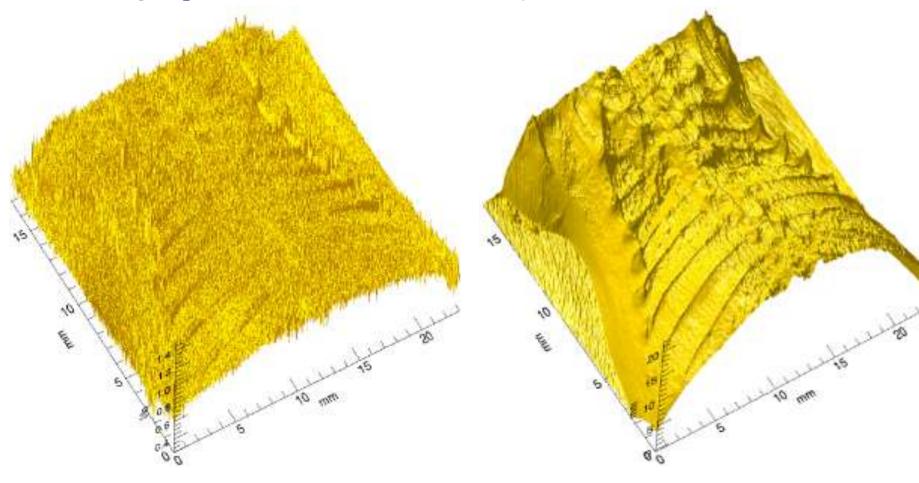
 $\nabla_{\perp} \cdot (I(\mathbf{r}_{\perp}, z) \nabla_{\perp} \phi(\mathbf{r}_{\perp}, z)) = -\frac{2\pi}{\lambda} \frac{\partial}{\partial z} I(\mathbf{r}_{\perp}, z)$ Solve for object's projected thickness using Fourier **Derivative Theorem**

$$T(\mathbf{r}_{\perp}) = -\frac{1}{\mu} \ln \left(\mathbf{F}^{-1} \left\{ \mu \frac{\mathbf{F} \left\{ M^{2} I(M\mathbf{r}_{\perp}, z = R_{2}) \right\} / I_{O}}{MR_{2} \delta \left| \mathbf{k}_{\perp} \right|^{2} + \mu} \right\} \right)$$

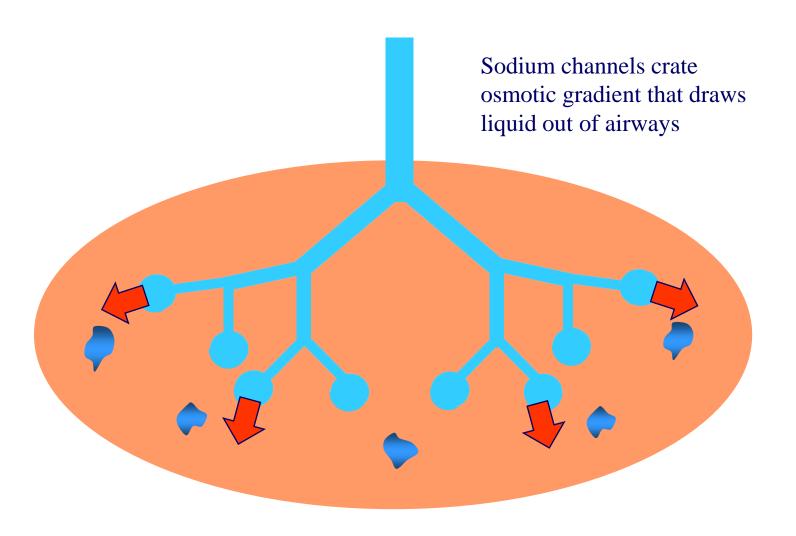
Phase to Projected Thickness

Phase image R_2 =4.26m, E=33keV

Projected thickness



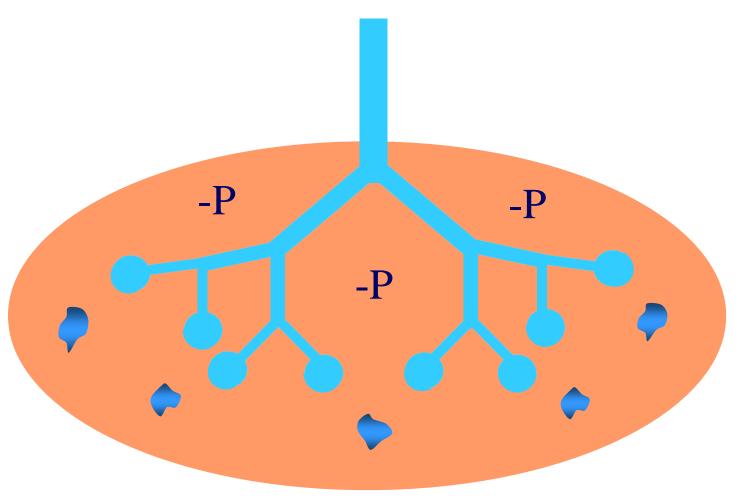
Lung aeration: Airway liquid clearance



Breathing Aerates Lungs 20 -∆ lung volume (mL/kg) b 15 -10 -5 _ 0 . 15 20 25 30 35 10 Time (secs) (a) (b)

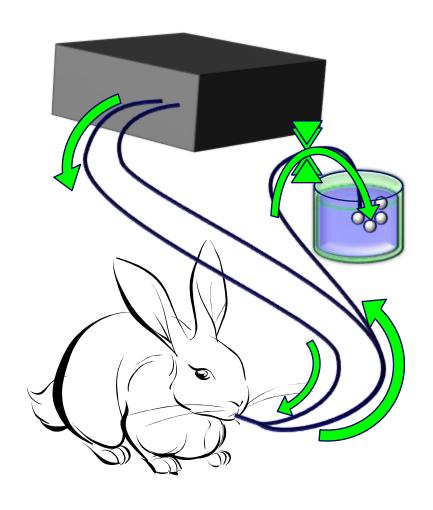
Lung aeration: Airway liquid clearance

Inspiration forces liquid out of airways

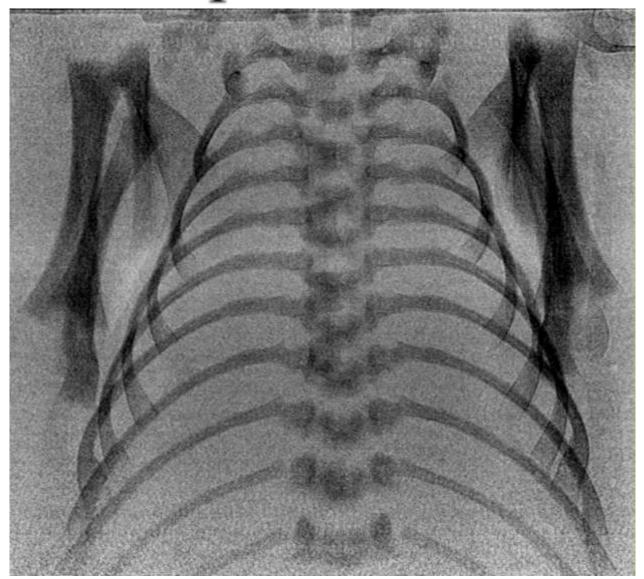


Medical Relevance

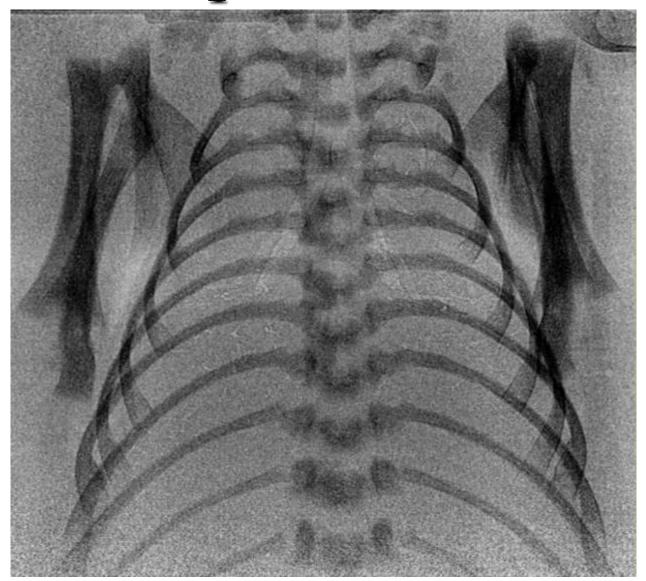
- Respiratory Ventilation
- Positive End Expiratory
 Pressure (PEEP) is used in some hospitals as it is thought to help
- It is currently excluded from international resuscitation guidelines for ventilating infants due to lack of evidence



Rabbit Pup: No PEEP

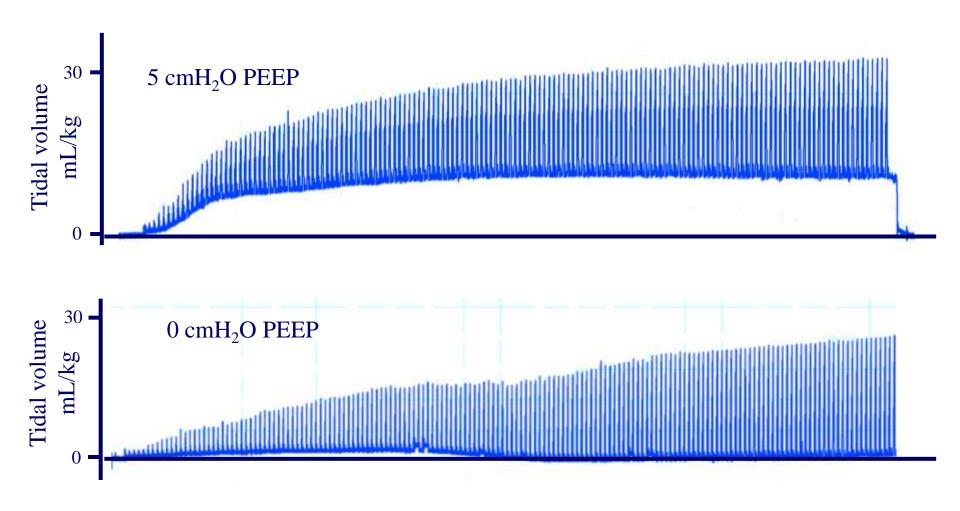


Rabbit Pup: With PEEP

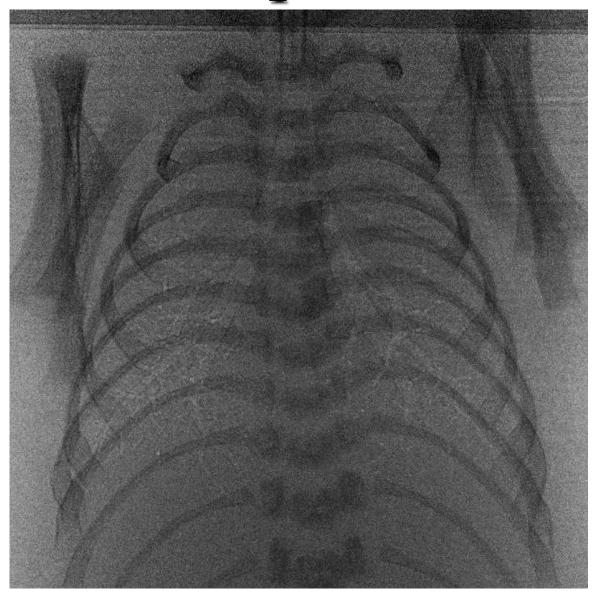


Te Pas et al Pediatric Research **65**(5), 537-541 2009 S. Hooper et al FASEB **21**, 3330 (2007)

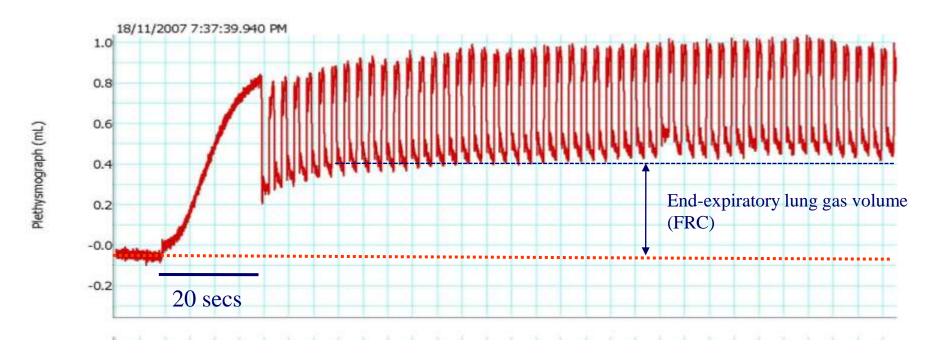
Effect of PEEP in Ventilated Preterm Rabbits



20sec First Inspiration



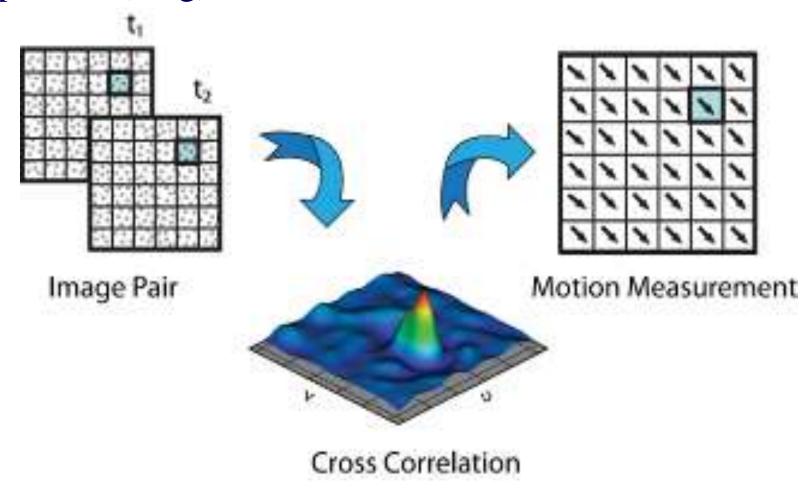
Long First Inspiration



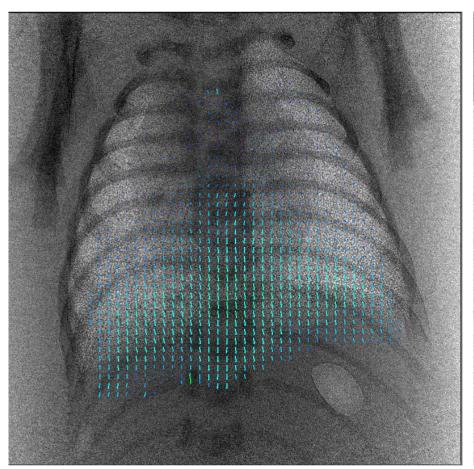
20 sec long inspiration 5 cmH₂O PEEP

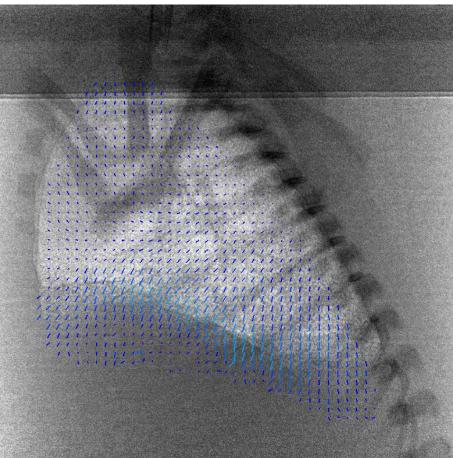
Measuring Lung Motion

■ Particle Image Velocimetry detects speed & direction of particle (lung) motion



Particle Image Velocimetry





Disease Detection

Plots of regional compliance, calculated from motion maps in mouse lungs



Healthy Lung, showing uniform compliance



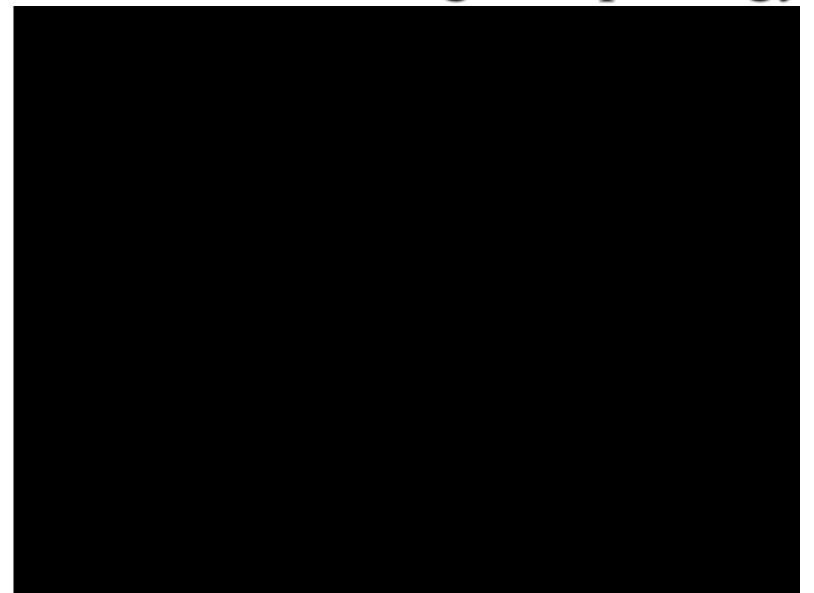
Fibrotic lung, showing regional differentiation of compliance

Moving to 4 Dimensions

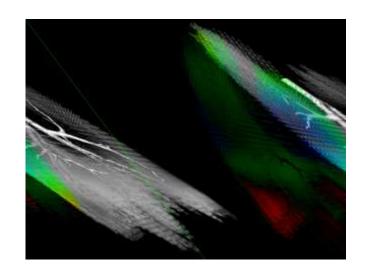
- Use controlled repeated breaths and rotate animal
- Select same point in breath for each rotation angle of animal
- Reconstruct CT image for each point in the breath



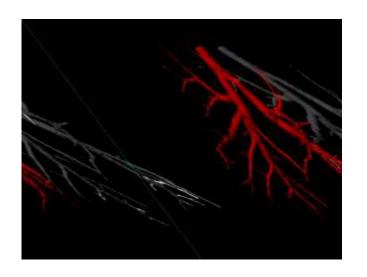
Whole Breath Lung Morphology



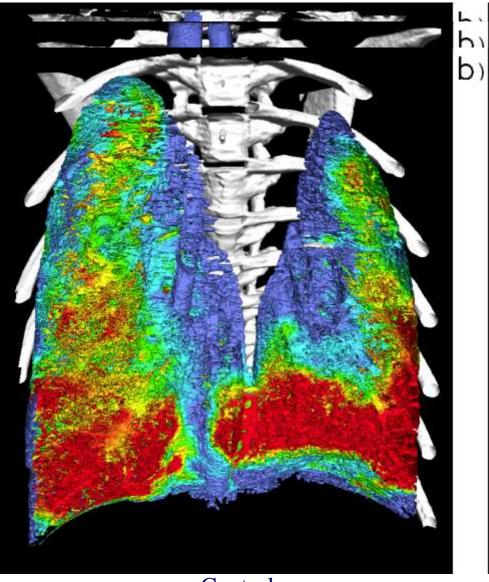
4D PIV

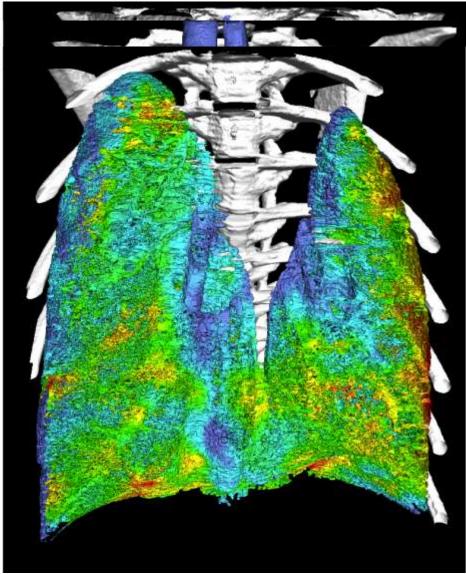


4D Flow



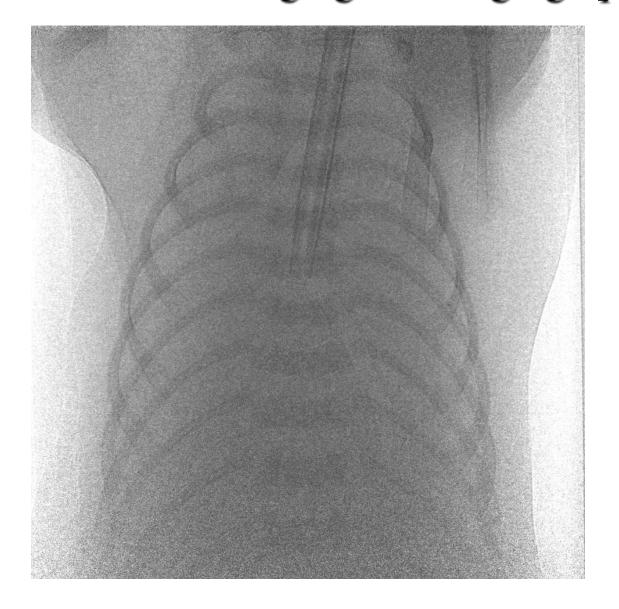
Asthma — detecting bronchoconstriction







Simultaneous Phase Imaging and Angiography



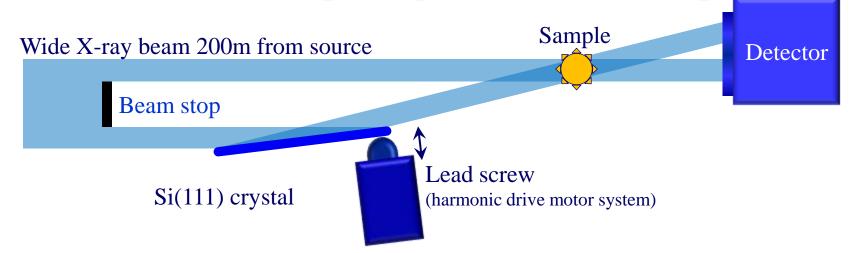
Videos used to train Doctors

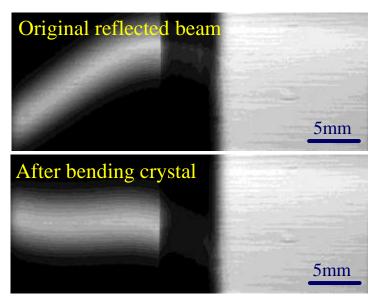


Major Issues: Technical

■ Static beam greatly limits 4D imaging (x, y, z, t)

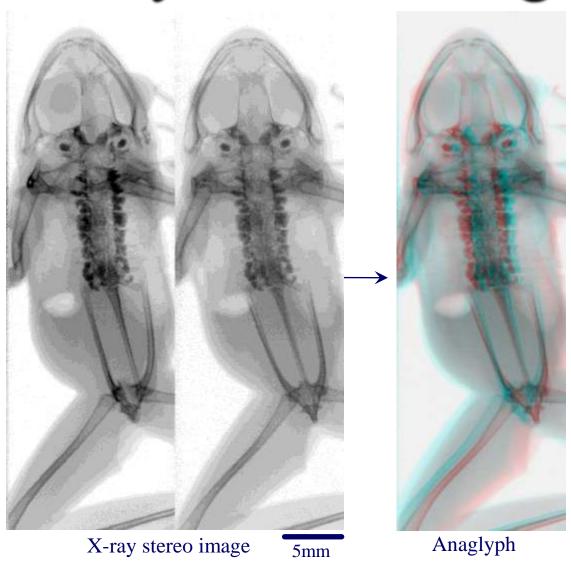
Stereo imaging at SPring-8





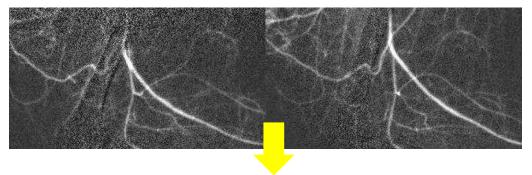
- Distorted reflected beam a result of...
 - Vertical energy dispersion of monochromator
 - Vertical and horizontal spread of X-ray beam.
 - Deformation of first crystal in monochromator by heat load
- Corrected by
 - Bending silicon crystal by pushing one end with screw while keeping the other end fixed (see figure)

X-ray Stereo Imaging



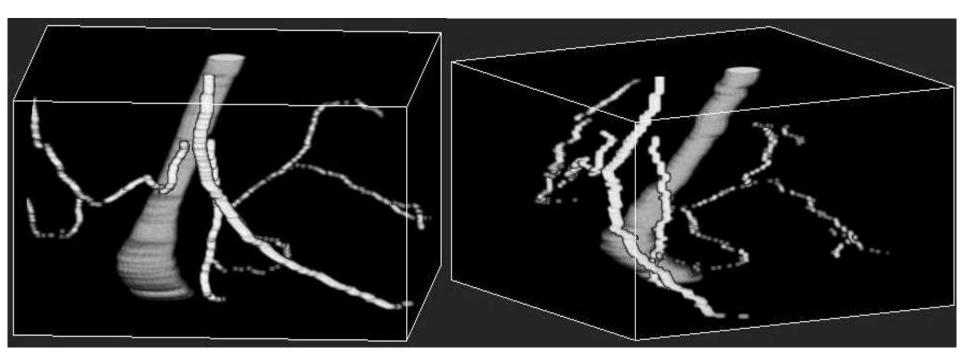
- Live Frog (*Rana* japonica)
- CCD Frame rate: 20Hz
- X-ray energy: 15keV
- Sequential images were acquired whilst vertically translating sample
- The images were combined digitally

Time-Resolved 3D Imaging



The three-dimensional arrangement of femur and blood vessels was estimated from X-ray stereo angiography.

The 3D quality is far from X-ray CT but sub-second time resolution possible



Radiotherapy

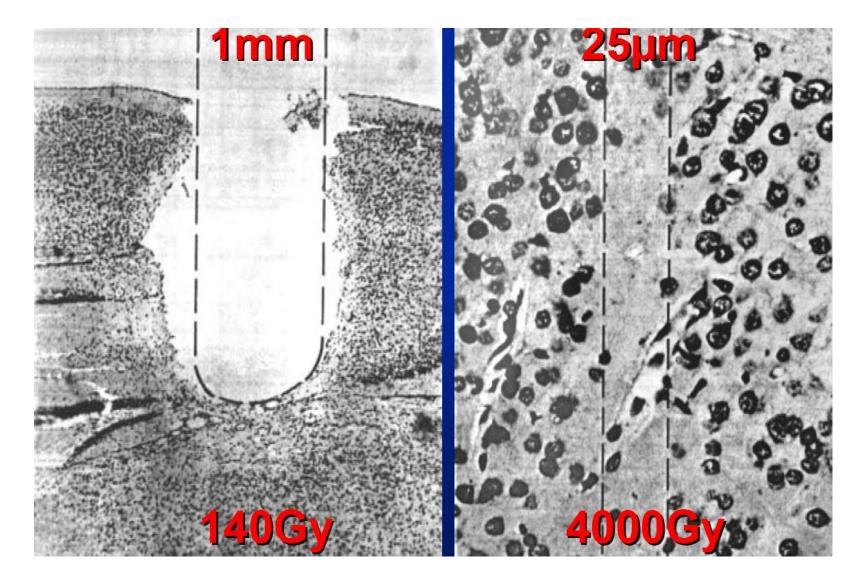
- The tumour can always be destroyed......
- ...If we give it enough dose
- The question is.....
- ...Can we keep the patient alive and healthy whilst we do it?
- The radiation dose we can give to the tumour is limited by.....
- ..How much dose healthy tissue can tolerate whilst we try to zap the tumour

Radiotherapy

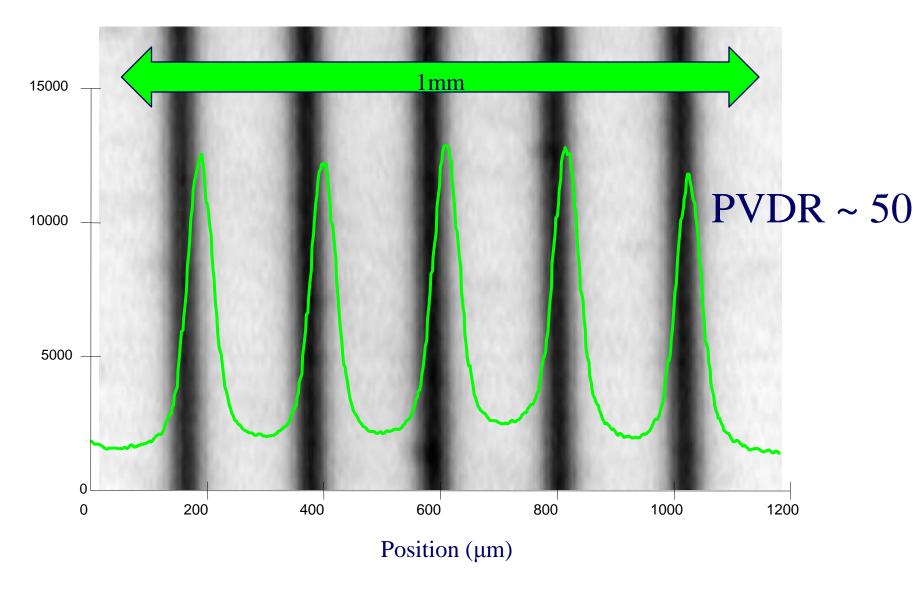
- The radiation dose that can be delivered to the tumour is limited by.....
- ..The tolerance of the surrounding healthy tissue
- Conventional Therapy
 - Uses a LINAC (high energy Xrays several MeV)
 - Uniformly irradiates tumour



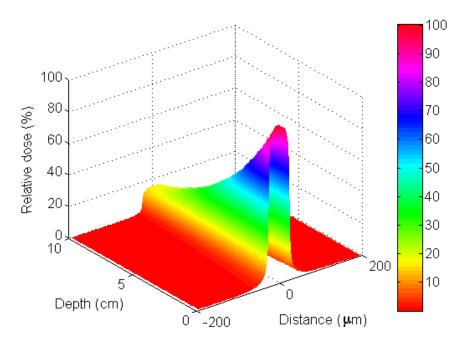
Deuteron Beam: Mouse Visual Cortex



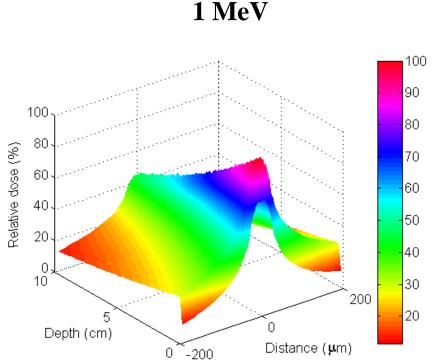
Peak to Valley Ratios



Dose Depth Curves



Synchrotron Spectrum (~100keV)



Loss of Pattern with Depth

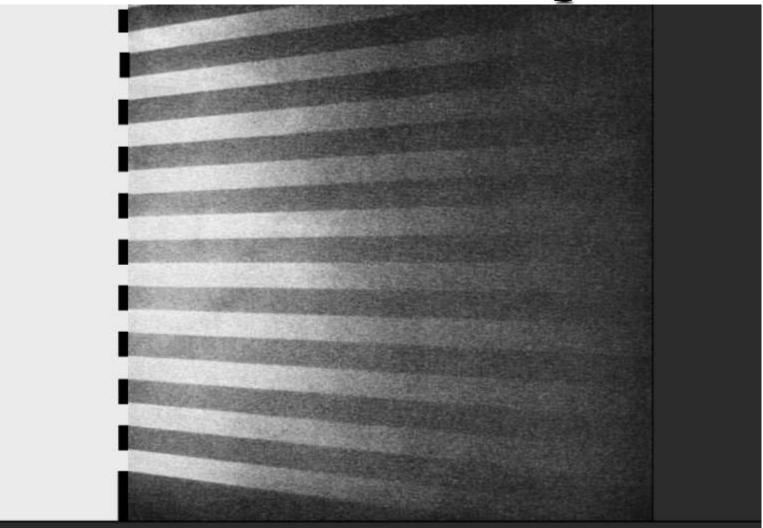
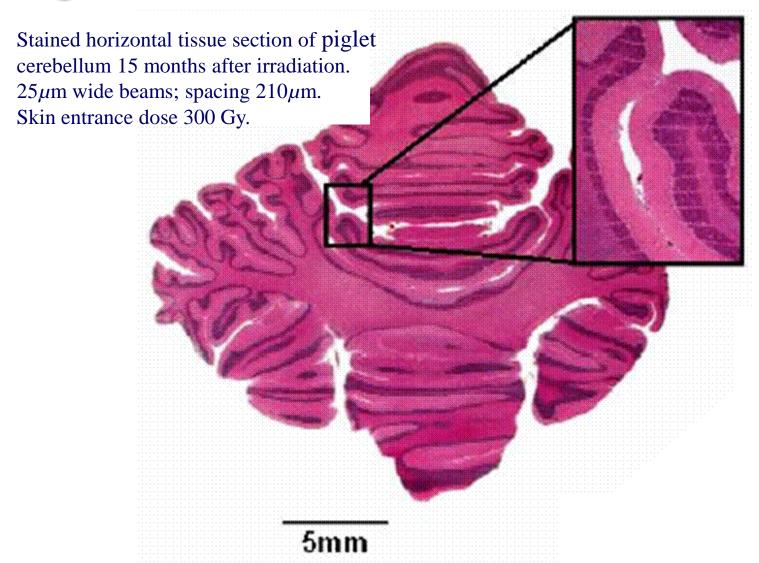


Fig. 43. Shafts of radiation through sieve fields showing divergence and obliteration of sieve pattern in depth

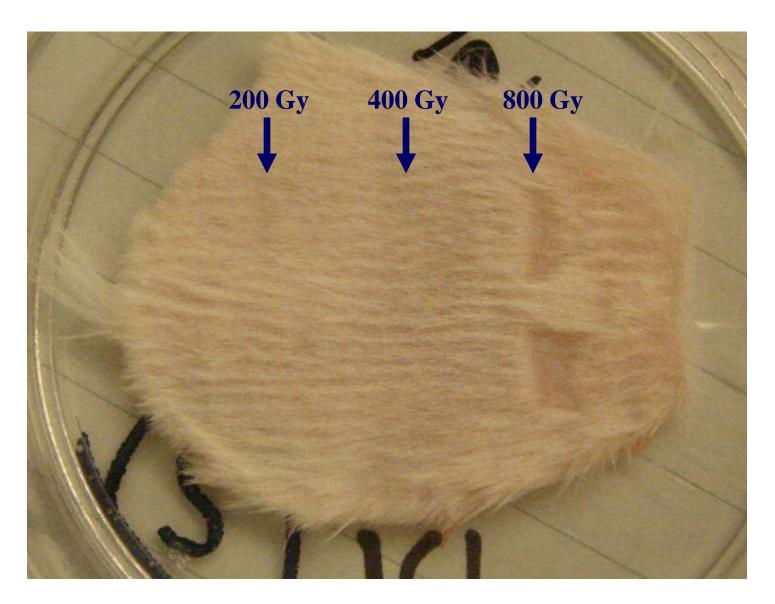
Piglets



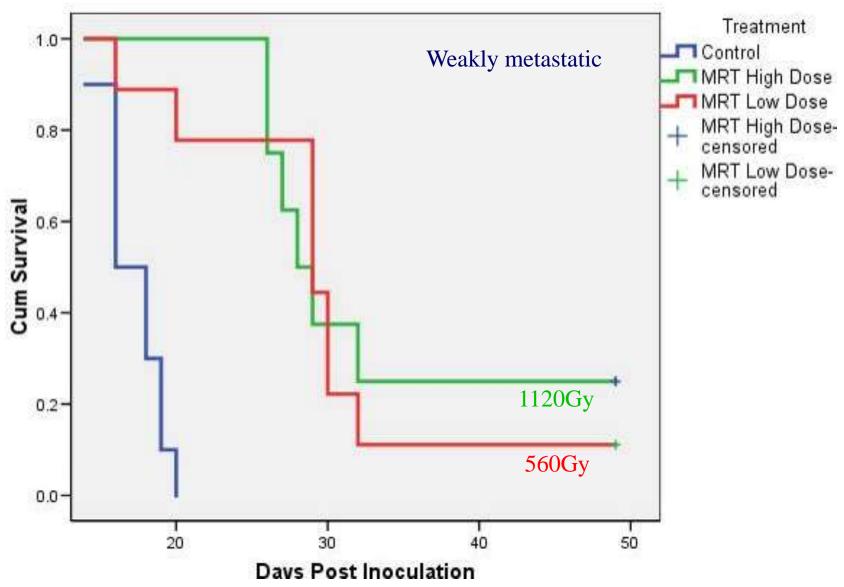
MRT on Mice

- Radiobiology of MRT is not well understood
- An understanding of the radiobiology is crucial for the optimisation of MRT and for any clinical implementation
- Understanding MRT will also inform conventional radiotherapy
- Mice are by far the best characterised mammal
 - ♦ Many GM mouse models already available
 - Many assays have been developed

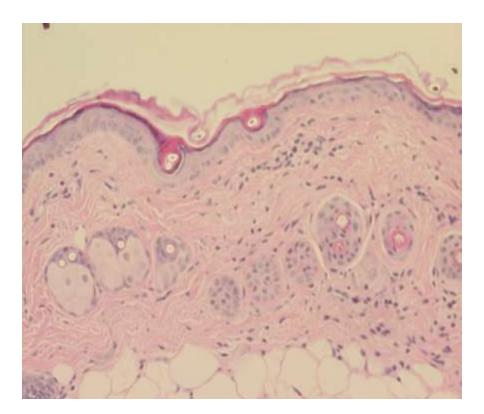
Exfoliation

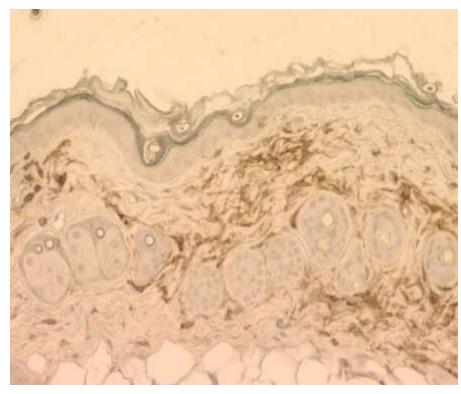


Survival Fractions EMT 6.5



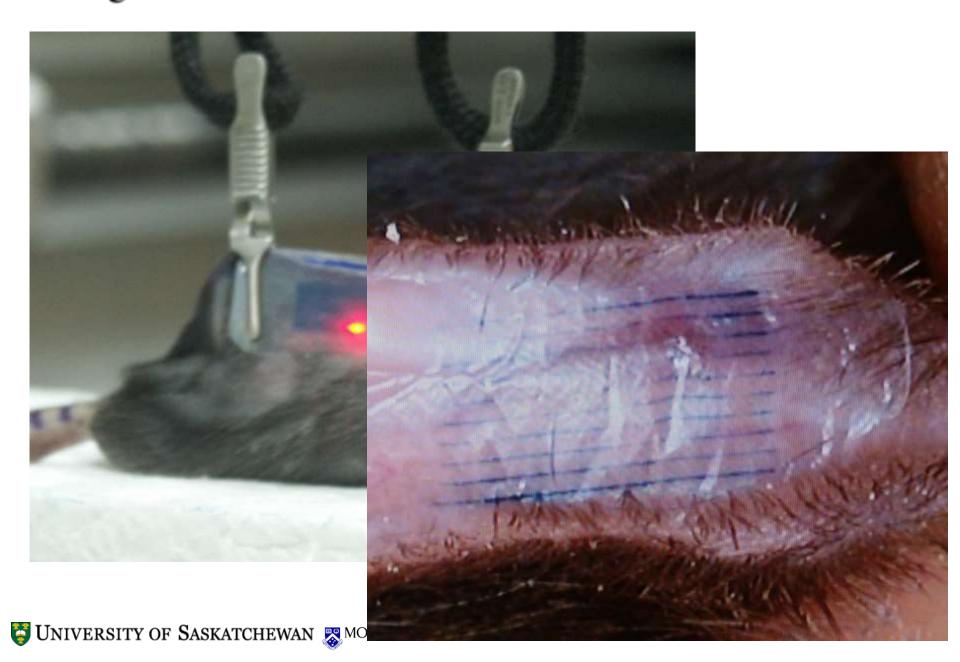
Results - Immunohistochemistry



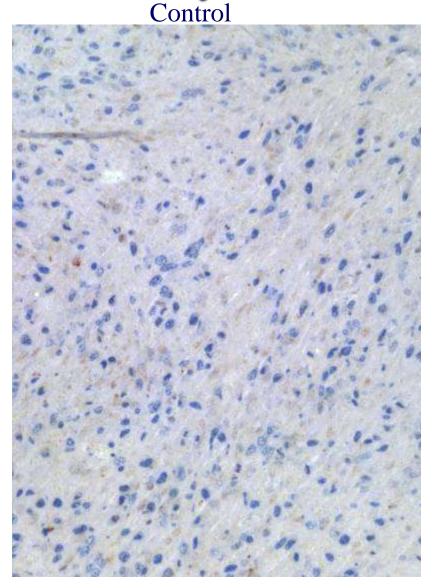


- H&E and CD45 Leukocyte Common Antigen (LCA) Staining of MRT-irradiated Mouse skin 5.5 days PI (x 100)
- Intact hair follicles & sebaceous glands

Using Radiochromic Film to Locate Microbeams

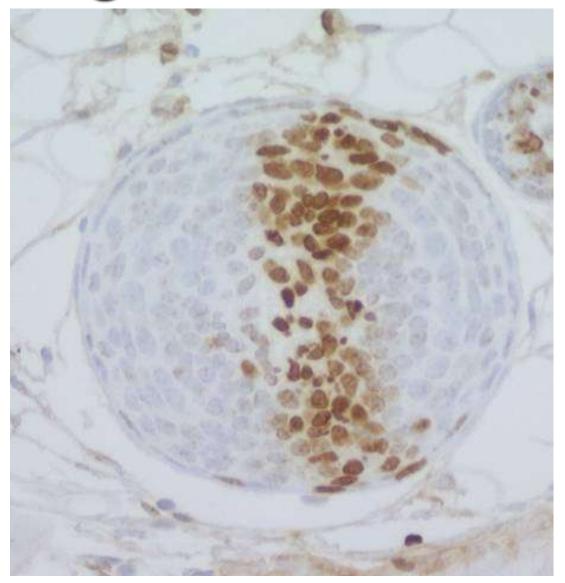


γH2AX/BrdU IHC post 560 Gy MRT treated Control



48 hours after irradiation

Splitting Hairs!



Conclusions

- X-rays are here for a while
- Synchrotrons have an important role in developing new x-ray methods in medicine
- In order to translate the research into the clinic, some human studies are necessary
- Much can be achieved with animal studies

The Team

- Stuart Hooper
- Megan Wallace
- Marcus Kitchen
- Melissa Siew
- Beth Allison
- Andreas Fouras
- Karen Siu
- Arjan te Pas
- Chris Hall
- Naoto Yagi
- Kentaro Uesugi
- Kaye Morgan
- Sally Irvine
- David Parsons
- Peter Rogers
- Jeff Crosbie

